SmartArch Multi-Force Superelastic Archwires: A New Paradigm in Orthodontic Treatment Efficiency

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O rthodontic manufacturers are currently focused on developing technologies that will accelerate treatment and reduce overall treatment times. Although clinicians have access to a variety of appliances and wires designed to meet the demand for faster treatment, these advanced products, if used incorrectly, can actually slow the rate of tooth movement. The SmartArch* multi-force archwire is a new technology that can both accelerate treatment and, more important, improve clinical efficiency in treating malocclusions.

Acceleration means increasing the rate of progression toward a specific goal. Efficiency means employing the least effort possible to progress toward an end goal. This is the true definition of simplification. Our goal as orthodontists should be to increase efficiency rather than accelerate treatment, because if efficiency is improved, accelerated treatment will follow.

Achieving greater efficiency requires an indepth understanding of technology and biology. Technology applied inappropriately or biology interpreted incorrectly will result in inefficient tooth movement and prolonged treatment times. This article discusses advanced wire technology and biological principles of tooth movement, illustrating the use of the SmartArch system in two cases.

Mechanical and Biological Considerations

Nickel titanium archwires have been evolving since their initial development in the early 1960s,¹⁻¹⁶ with Copper NiTi** introduced in the early 1990s. Superelastic wires are most commonly used with preadjusted appliances for initial leveling and alignment; finishing and detailing are typically accomplished with TMA* or stainless steel arch-

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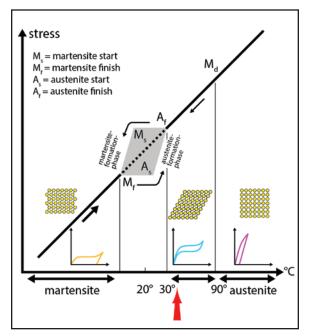


Fig. 1 During stress-related transition from martensitic to austenitic phase, optimal superelastic properties occur at body temperature (red arrow).

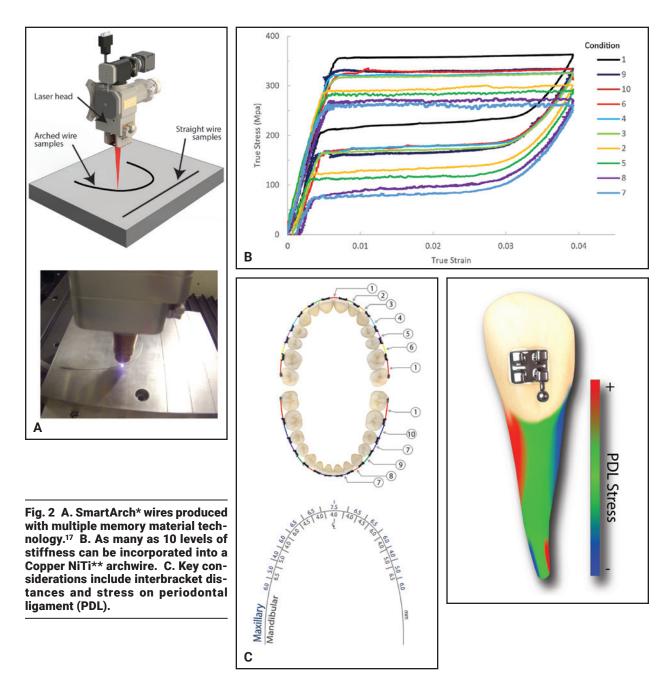
wires, since 1st-, 2nd-, and 3rd-order bends cannot be placed in nickel titanium wires.

The superelasticity of nickel titanium wires is achieved through stress-related martensiteaustenite transformation (Fig. 1).¹⁷ Nickel titanium wires do not exhibit superelastic behavior at deflections of less than about 1mm.¹⁸ Exposing nickel titanium wire to a sharp deformation while the wire is in its cold martensitic condition will result in permanent wire deformation.¹⁸

The three methods currently used to program these wire transformation phases are furnace heating, holding, and cooling; pulsed electric current from a Memory Maker***¹⁸; and pulsed fiber laser conditioning.†¹⁹ SmartArch wires are manufactured by the third method—known as multiple memory material technology—which precisely programs transition zones as narrow as .001" in a cross-section of shape-memory alloy wire. For example, 10 separate superelastic unloading zones can be programmed into a Copper NiTi wire (Fig. 2).¹⁷

Orthodontic anchorage techniques are based

on the understanding that posterior teeth are larger than anterior teeth and maxillary teeth are larger than mandibular teeth. Larger teeth are more resistant to movement because of increased periodontal ligament (PDL) and root support. Therefore, a threshold of stress must be achieved before a biological response will cause tooth movement. Too little stress results in less tissue alteration and less attraction of osteoclasts, leading to slower tooth movement. Conversely, too much stress re-



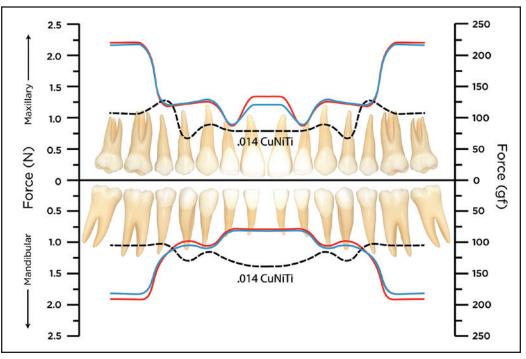


Fig. 3 Comparison of ideal force²⁰ (red line) and forces delivered by traditional nickel titanium archwires (dotted line) and SmartArch archwires (blue).

sults in necrosis of the PDL tissue. Ideally, the application of appropriate force levels over an extended period will result in efficient tooth movement.

Viecilli and Burstone studied the effective force levels on average-size teeth in each arch to determine the appropriate level of force required to achieve an optimal biological response for each tooth.²⁰ Their study focused on four common orthodontic movements: translation, tipping, rotation, and extrusion. SmartArch archwire programming was based on specific PDL compressive stress values derived from Viecilli and Burstone's finite element modeling of digital dental templates. The result is an archwire with seven specific zones preprogrammed to apply appropriate forces to each individual tooth, both maxillary and mandibular.

Orthodontists have traditionally chosen starting archwires based on their ability to insert the wire comfortably into the patient's mouth. Considering the force levels found in Viecilli and Burstone's analysis, however, the .014" Copper NiTi archwire typically used to begin treatment underpowers the maxillary arch and overpowers the mandibular anterior segment. In short, our most common starting archwire provides too little force in the upper arch and overstresses the lower anterior teeth (Fig. 3).

As explained by Reitan, when a stress is applied to a tooth, tipping will occur until the PDL is compressed, halting tooth movement.²¹ The second phase, or lag phase, is characterized by the formation of avascular hyalinized tissue. Once the avascular hyalinized tissue has been removed, more or less continuous tooth movement occurs in a frontal resorptive pattern, completing the second phase. This undermining resorption phase may be as short as four to five days or as long as 10 weeks, depending on the amount of avascular hyalinized tissue. Each time a force is applied or changed, the

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body responds with some degree of avascular hyalinized tissue formation. The orthodontist's goal should be to apply enough force to activate the biological response and begin tooth movement, while maintaining as light a force as possible to minimize the formation of avascular necrotic tissue. Enough force must be continuously applied to maintain the frontal resorptive pattern once the lag phase has been completed. The result of this process is efficient tooth movement.

A final point is that orthodontic tooth movement is accomplished with both determinate and indeterminate mechanics. Determinate mechanics are more predictable because all the three-dimensional forces and moments are known.¹⁷ Any device engaging more than two abutments results in indeterminate loads on the PDL, causing greater PDL necrosis and inefficient tooth movement. Hence, the more determinate the mechanics, the more efficient the treatment.

SmartArch archwires deliver physiologically optimized forces over an extended period. With carefully applied orthodontic mechanics, SmartArch wires can shorten the lag phase, reduce adjustment and reactivation requirements, and avoid indeterminate mechanics, thus increasing orthodontic efficiency. An ideal treatment sequence begins with an .016" SmartArch Copper NiTi wire, moves into an .018" \times .025" SmartArch Copper NiTi wire, moves into an .018" \times .025" SmartArch Copper NiTi wire, moves steel archwires. The current objective is to develop protocols for treating the majority of cases in 12 months or less.

Basic considerations involved in SmartArch diagnosis, treatment planning, and biomechanics include the following.

Wire placement: Bend the archwire to create stress-induced martensitic transformation. Any type of mild to moderate (1-3mm) bend will suffice. Avoid sharp bends that cause permanent deformation and wire breakage.

Patience: Let the wire work. Allow time for the lag phase to finish and frontal absorption to take over. Any removal or adjustment of the wire causes a reversion to the lag phase. Resist the tendency to adjust too frequently.

Whole arch: Bond as many teeth as possible, in-

cluding second molars and blocked-out teeth, right from the start. This allows the biology to work consistently across the entire arch.

Orthodontists will need to shift their paradigm from an "adjust at every appointment" (tinkering) mentality to an attitude of observing the body's response to the mechanics and allowing the technology to work. Overactivation of SmartArch wires reverts the patient into the lag phase, reducing efficiency and prolonging treatment.

Case 1

A 22-year-old female presented for treatment of minor crowding, a moderately deep bite, and narrow dental arches (Fig. 4). Examination found a lower midline shifted 2mm to the right; mild crowding in both arches; an asymmetrical, skewed upper archform; and lips that were slightly retrusive relative to the E-line (Table 1). A good facial profile and balance were noted, along with normal upper incisor positions and lingual tipping in the buccal segments. The molar and canine relationships were diagnosed as Class I on the left and one-fourth- to one-half-unit Class II on the right.

Treatment goals were to resolve the deep bite, broaden and enhance both arches, correct the asymmetrical maxillary archform, and finish with Class I molar and canine relationships. The estimated treatment time was 18 months.

Damon Q** brackets were bonded to all teeth in both arches: low-torque brackets on the upper and lower incisors, high-torque brackets on the lower canines, and standard brackets on all other teeth (Fig. 5). Anterior bite turbos were bonded to the lingual aspects of the upper central incisors. SmartArch .016" Copper NiTi archwires were inserted in all brackets, with no elastics worn at the start.

After five weeks of treatment, the upper right second molar was rebonded, and maxillary and mandibular archwires were changed to $.018" \times .025"$ SmartArch Copper NiTi (Fig. 6). The turbos remained in place.

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A new panoramic x-ray was taken after 13 weeks of treatment, and the brackets were repositioned on the upper left central and lateral incisors, the upper right lateral incisor, and the lower right first molar.

After 20 weeks of treatment, the turbos were removed and Class II elastics ($5/16^{"}$, 2oz) were prescribed for full-time wear. The upper canine brackets were replaced with high-torque brackets, and elastic thread was placed across the four upper

	Norm	Pretreatment	Post-Treatment
SNA	82.0°	76.2°	76.2°
SNB	80.0°	74.7°	74.7°
ANB	2.0°	1.5°	1.4°
FMA	26.0°	16.3°	14.0°
MP-SN	33.0°	30.6°	33.0°
U1-APo	6.0mm	2.1mm	2.7mm
L1-APo	1.0mm	0.5mm	-0.2mm
U1-PP	110.0°	98.9°	103.5°
IMPA	95.0°	94.6°	90.7°

 TABLE 1

 CASE 1 CEPHALOMETRIC ANALYSIS

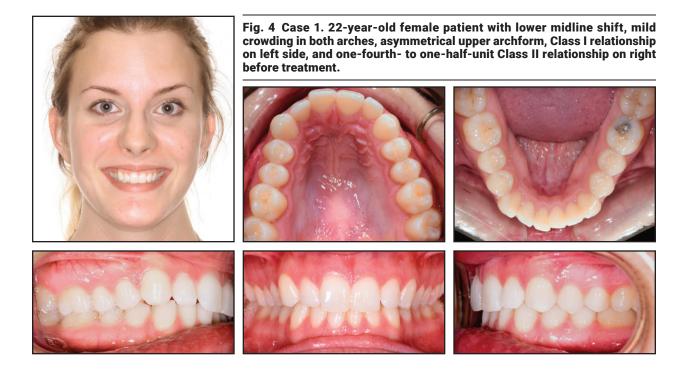






Fig. 5 Case 1. Damon Q** brackets bonded and .016" SmartArch Copper NiTi wires placed in both arches.





Fig. 6 Case 1. After five weeks of treatment, .018" × .025" SmartArch Copper NiTi wires placed in both arches.





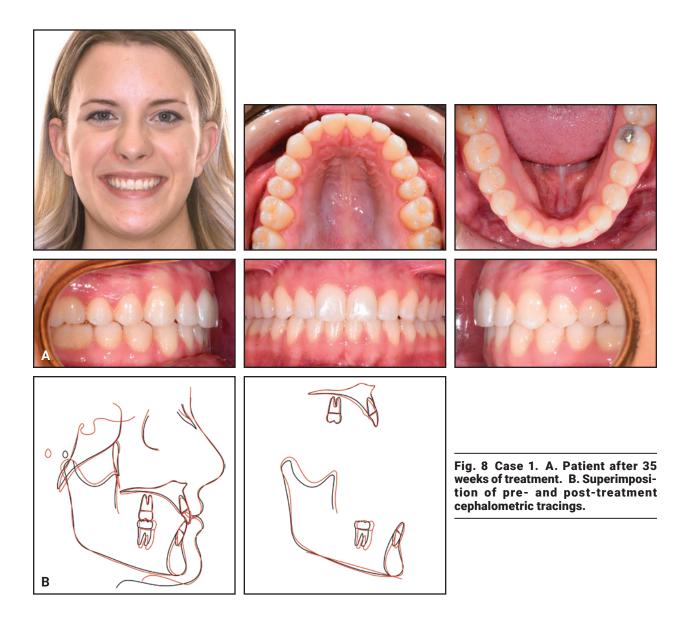
Fig. 7 Case 1. After 25 weeks of treatment, stainless steel finishing wires placed in both arches.

incisors to consolidate space.

After 25 weeks of treatment, an .019"× .025" stainless steel archwire with steel posts between the lateral incisors and canines was placed in the maxillary arch, with a stainless steel ligature wire tied across the upper incisors (Fig. 7). An .016" × .025" stainless steel archwire with posts was placed in the mandibular arch. The patient was instructed to continue wearing the elastics.

The archwires were expanded after 29 weeks of treatment, and finishing and detailing bends were made to upright the lower left premolars. The Class II elastic was discontinued on the left side only, and a midline elastic was started from the lower right canine to the upper left canine. The archwires were recoordinated and expanded further after 33 weeks, with a finishing bend added for the lower right first premolar.

Fixed appliances were removed after a total treatment time of 35 weeks. Because the patient preferred Memotain‡ fixed retainers, a TRIOS†† scan was taken for fabrication of 2-2 maxillary and 3-3 mandibular retainer wires. In-house clear overlay retainers were delivered for full-time wear un-



til the Memotain retainers could be bonded, four weeks later. Maxillary and mandibular Prezurv‡‡ clear overlay retainers were then delivered for nighttime wear.

Post-treatment records demonstrated good dental alignment, proper seating, and functional occlusion (Fig. 8, Table 1). An appropriate overbite was established, and the buccal segments were uprighted and expanded, resulting in a beautiful, broad smile. The maxillary arch asymmetry was corrected.

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^{‡‡}Trademark of AOA Orthodontic Appliances, Sturtevant, WI; www.aoalab.com.

Case 2

A 12-year-old female presented for treatment of minor crowding, a moderately deep bite, and narrow dental arches (Fig. 9). The examination showed an upper midline shifted 1mm to the left, moderate crowding in both arches, unilateral crossbites of the upper left lateral incisor and upper right first premolar, and lips that were slightly protrusive relative to the E-line. Good facial profile and balance were noted. The upper incisor positions were normal, but the buccal segments were lingually tipped. The patient was diagnosed with bilateral Class I molar and Class II canine relationships.

Our nonextraction treatment plan was to use Insignia* custom braces with anterior bite turbos and SmartArch .016" and .018" \times .025" Copper NiTi archwires, followed by .021" \times .025" Insignia custom Copper NiTi and .021" \times .025" TMA wires. The goals were to level and align the dentition and correct the midline discrepancy.

Fixed appliances were bonded to all teeth in both arches, and .016" SmartArch Copper NiTi

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wires were placed (Fig. 10). Anterior bite turbos were bonded as in Case 1.

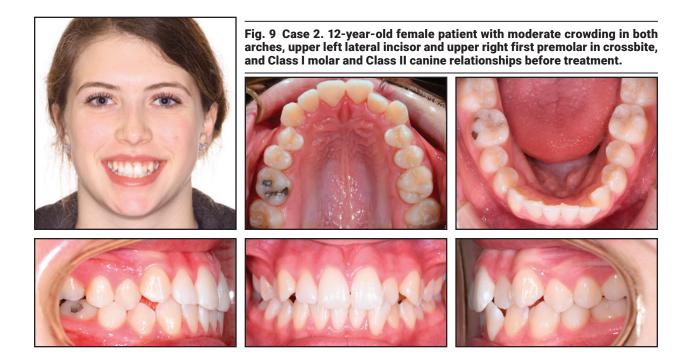
After 10 weeks of treatment, the crowding was resolved, crossbites were corrected, and midlines were coincident, but slight rotations remained (Fig. 11). New .018" \times .025" SmartArch Copper NiTi wires were placed in both arches.

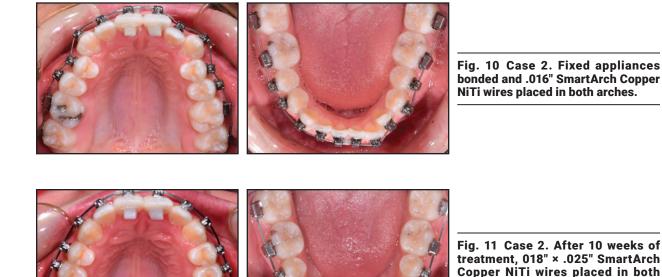
After 20 weeks of treatment, the rotations were corrected and proper alignment was achieved (Fig. 12). The bite turbos were removed, and .021" \times .025" Insignia custom Copper NiTi archwires were placed for finishing in both arches.

Discussion

Case 1 demonstrates the efficiency that can be achieved when archwire technology is applied appropriately. Because the wires were allowed to express themselves without being removed and adjusted, we avoided the tendency to revert from a frontal resorptive pattern back into the lag phase, and the arches developed in a timely fashion.

The patient's response to the SmartArch archwires was consistent with what I expected





from an arch-development standpoint (Table 2). Still, a few subtle adjustments could have led to even greater clinical efficiency. The $.018" \times .025"$ archwires were placed at five weeks because of the loss of the upper right second molar bracket. I believe less undermining resorption would have been required if the initial archwire had been allowed another three weeks to work, potentially saving four to five weeks of treatment time. In addition, hooks were placed on the upper canines at 20 weeks for attachment of Class II elastics. This created an indeterminate mechanical situation, in which the amount and location of hyalinized PDL could not be determined. A better clinical approach might have been to wait for the posted stainless steel wires to be placed, thus creating a more efficient determinate system, before initiating elastic wear. An additional benefit noted in this case was

An additional benefit noted in this case was the lack of patient discomfort during treatment. Although every individual is different when it comes to pain, this patient's only reported discomfort occurred when the elastic thread was placed. Case 2 illustrates the combined efficiency of

Case 2 illustrates the combined efficiency of the SmartArch and Insignia systems. Accurate bracket placement, with appropriate forces applied to each tooth, created a synergistic biological response. We were able to insert finishing archwires for detailing and occlusal refinement after only five months of treatment.

arches.

TABLE 2 CASE 1 ARCH EXPANSION FROM PRETREATMENT TO 25 WEEKS*

	Maxillary	Mandibular
Canines	+2.24mm	+2.57mm
First premolars	+4.21mm	+4.11mm
Second premolars	+3.38mm	+3.45mm
First molars	+1.66mm	+1.62mm
Second molars	+0.43mm	+0.38mm

*Recorded and measured from digital scans; 25 weeks = removal of .018" × .025" archwires and start of finishing phase.









Fig. 12 Case 2. After 20 weeks, SmartArch treatment completed, bite turbos removed, and Insignia* treatment started.

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Conclusion

The conventional wire progression—stepping through multiple rounds of progressively greater size and force—results in forces that overpower some teeth and underpower others. The value of this new wire technology lies in its capacity to apply physiologically appropriate forces to each individual tooth, thereby minimizing the formation of avascular necrotic tissue and shortening the lag phase. In each case shown here, SmartArch treatment appeared to minimize the lag phase, making coordinated tooth movement more efficient and leading to an estimated 50% savings in leveling and alignment time.

Based on the cases I have treated so far, it appears the best time to initiate treatment with these wires is upon full eruption of the second molars. Although SmartArch can be used with any bracket system, taking full advantage of the technology requires thoughtful treatment planning, accurate bracket placement, and careful observation before manipulating the bracket-wire system.

REFERENCES

- Bennett, J.C. and McLaughlin, R.P.: Orthodontic Treatment Mechanics and the Preadjusted Appliance, Wolfe Publishing, London, 1993.
- Clement, R.; Geiger, M.; Schneider, J.; and Sander, F.G.: Heat treatment of NiTi shape memory alloys by electric current, in *Computer Methods in Biomechanics and Biomedical Engineering*, vol. 4, University of Wales College of Medicine, Cardiff, United Kingdom, 2002.
- Faltin, R.M.: Torsionsverhalten und Beeinflussung von NiTiund NiTi-Stahl-Materialien in der Kieferorthopädie [in German], dissertation, University of Ulm, Germany, 1998.
- 4. Hempowitz, H.: Analyse kieferothopädischer Problemstellungen mit Hilfe der Methode der Finiten elemente [in German], dissertation, University of Ulm, Germany, 1999.
- Jarabak, J.R. and Fizzell, J.A.: *Technique and Treatment with* Light-Wire Edgewise Appliances, 2nd ed., Mosby, St. Louis, 1972.
- Linge, L. and Dahm, S.: The practical aspects of using "superelastic" arch wires in the edgewise technic, J. Orofac. Orthop. 55:324-329, 1994.
- McNamara, J.A. and Brudon, W.L.: Orthodontic and Orthopedic Treatment in the Mixed Dentition, Needham Press, Ann Arbor, MI, 1993.
- Meling, T.R. and Odegaard, J.: The effect of short-term temperature changes on super elastic nickel-titanium archwires activated in orthodontic bending, Am. J. Orthod. 119:263-273, 2001.

- Miura, F.; Mogi, M.; Ohura, Y.; and Hamanaka, H.: The super elastic property of the Japanese NiTi alloy wire for use in orthodontics, Am. J. Orthod. 90:1-10, 1986.
- Miura, F.; Mogi, M.; and Ohura, Y.: Japanese NiTi alloy wire: Use of the direct electric resistance heat treatment method, Eur. J. Orthod. 10:187-191, 1988.
- Proffit, W.R.: Contemporary Orthodontics, Mosby, St. Louis, 1986.
- 12. Ricketts, R.M.; Bench, R.W.; Gugino, C.F.; Hilgers, J.J.; and Schulhof, R.J.: *Bioprogressive Therapy*, Rocky Mountain Orthodontics, Denver, 1979.
- Sakima, M.T.; Dalstra, M.; and Melsen, B.: How does temperature influence the properties of rectangular nickel-titanium wires? Eur. J. Orthod. 28:282-291, 2006.
- Sander, F.G.: Eigenschaften superlasticher Drähte und deren Beeinflussung [in German], Inf. Orthod. Kieferorthop. 4:501-514, 1990.
- 15. Wichelhaus, A. and Sander, F.G.: Das Verhalten von superelastichen Drähten im elastischen und plastischen Bereich in

Abhängigkeit von der Temperatur [in German], Kieferorthop. Mitt. 8:95-106, 1994.

- Wichelhaus, A.: Die Entwicklung und klinische Anwendung superelastischer Bögen und Teibögen in der Kieferorthopädie [in German], dissertation, University of Ulm, Germany, 1995.
- Roberts, W.E.; Roberts, J.A.; Tracey, S.; and Sarver, D.M.: SmartArch multi-force, super-elastic archwires: A new paradigm in orthodontics, J. Digit. Orthod. 55:66-79, 2019.
- Sander, F.M.; Sander, C.; Roberts, W.E.; and Sander, F.G.: Bending properties of superelastic nickel titanium archwires, J. Clin. Orthod. 17:581-585, 2008.
- Khan, M.I.; Pequegnat, A.; and Zhou, Y.N.: Multiple memory shape memory alloys, Adv. Eng. Mater. 15:386-393, 2013.
- Viecilli, R.F. and Burstone, C.J.: Ideal orthodontic alignment load relationships based on periodontal ligament stress, Orthod. Craniofac. Res. 18:S180-S186, 2015.
- Reitan, K.: Clinical and histologic observation on tooth movement during and after orthodontic treatment, Am. J. Orthod. 53:721-745, 1967.